

TECHNICAL REPORT

ISO
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Road vehicles — Anthropomorphic side impact dummy —

Part 4 :

Lateral shoulder impact response requirements to assess biofidelity of dummy

Véhicules routiers — Mannequin anthropomorphe pour essai de choc latéral —

Partie 4 : Caractéristiques de réponse de l'épaule à un choc latéral permettant d'évaluer la biofidélité d'un mannequin



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Foreword

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The main task of ISO technical committees is to prepare International Standards. In exceptional circumstances a technical committee may propose the publication of a technical report of one of the following types:

- type 1, when the necessary support within the technical committee cannot be obtained for the publication of an International Standard, despite repeated efforts;
- type 2, when the subject is still under technical development requiring wider exposure;
- type 3, when a technical committee has collected data of a different kind from that which is normally published as an International Standard ("state of the art", for example).

Technical reports are accepted for publication directly by ISO Council. Technical reports of types 1 and 2 are subject to review within three years of publication, to decide whether they can be transformed into International Standards. Technical reports of type 3 do not necessarily have to be reviewed until the data they provide are considered to be no longer valid or useful.

ISO/TR 9790-4, which is a technical report of type 3, was prepared by Technical Committee ISO/TC 22, *Road vehicles*.

ISO/TR 9790 consists of the following parts, under the general title *Road vehicles — Anthropomorphic side impact dummy*:

- *Part 1: Lateral head impact response requirements to assess biofidelity of dummy*
- *Part 2: Lateral neck impact response requirements to assess biofidelity of dummy*
- *Part 3: Lateral thoracic impact response requirements to assess biofidelity of dummy*
- *Part 4: Lateral shoulder impact response requirements to assess biofidelity of dummy*
- *Part 5: Lateral abdominal impact response requirements to assess biofidelity of dummy*
- *Part 6: Lateral pelvis impact response requirements to assess biofidelity of dummy*

Road vehicles — Anthropomorphic side impact dummy —

Part 4 :

Lateral shoulder impact response requirements to assess biofidelity of dummy

1.0 INTRODUCTION

The impact response requirement presented in this Technical Report is the result of a critical evaluation of data selected from experiments agreed to by experts as being the best and most up-to-date information available.

A single dynamic response requirement is defined for lateral loading of the shoulder. It is based on impact tests conducted by Association Peugeot-Renault using unembalmed cadavers (1). A second requirement is implicit in the lateral neck bending requirement that is based on Ewing et al (2) human volunteer data. In those sled tests, the dummy must mimic the human volunteer's shoulder reaction with the rigid vertical side board in order for the kinematics of its upper thoracic spine to meet the T1 response requirements. Note that the Ewing data may be incompatible with the APR data because the Ewing volunteers were tensed in anticipation of the shoulder loading while the APR cadavers were unembalmed making them quite flaccid.

2.0 SCOPE AND FIELD OF APPLICATION

This Technical Report is one of six reports that describe laboratory test procedures and impact response requirements suitable for assessing the impact biofidelity of side impact dummies. This Technical Report provides information to assess the biofidelity of lateral impact response of the shoulder.

*Numbers in parentheses denote papers listed in References, Section 5.0

3.0 ISO REFERENCES

ISO DP 9790-1 Road Vehicles - Anthropomorphic Side Impact Dummy - Lateral Head Impact Response Requirements to Assess the Biofidelity of the Dummy.

ISO DP 9790-2 Road Vehicles - Anthropomorphic Side Impact Dummy - Lateral Neck Impact Response Requirements to Assess the Biofidelity of the Dummy.

ISO DP 9790-3 Road Vehicles - Anthropomorphic Side Impact Dummy - Lateral Thoracic Impact Response Requirements to Assess the Biofidelity of the Dummy.

ISO DP 9790-5 Road Vehicles - Anthropomorphic Side Impact Dummy - Lateral Abdominal Impact Response Requirements to Assess the Biofidelity of the Dummy.

ISO DP 9790-6 Road Vehicles - Anthropomorphic Side Impact Dummy - Lateral Pelvis Impact Response Requirements to Assess the Biofidelity of the Dummy.

4.0 REQUIREMENT

4.1 Original Data

Researchers of the Association Peugeot-Renault subjected 4 cadavers to lateral impacts delivered to the shoulder by the flat end of a 23 kg rigid cylinder of 150 mm diameter (1). Each cadaver was seated on a horizontal hardwood surface with a vertical backrest. The impact was delivered laterally to the shoulder. The force of the impactor was recorded. Results of these tests are given in Appendix A.

4.2 Response Requirements

The original force-time curves of the impactor were normalized (see Appendix A) using the technique suggested by Mertz (3). The normalized force-time curves and the proposed response corridor are shown in Figure 1. The maximum normalized deflection should be between 34 and 41 mm.

4.3 Test Setup

A 23 kg rigid, 150 mm diameter cylinder with a flat impact face is required. The dummy is to be seated upright and the impactor adjusted to strike the dummy's shoulder laterally between 4.4 m/s and 4.6 m/s. The axis of the impactor is to be aligned with the center of the shoulder joint.

4.4 Instrumentation

Instrument the dummy to monitor acceleration of the thoracic spine. Record the force of the impactor. Force and acceleration measurements are to meet SAE Channel Class 1000 filter requirements.

4.5 Normalization Procedure

Determine the impulse by integrating the force-time curve. Calculate the effective mass using the following relationship,

$$M_e = \left[\int_0^T F dt \right] / (V_0) \quad (1)$$

where $\int_0^T F dt$ is the impulse and V_0 is the impact velocity. The mass ratio defined in Appendix A is,

$$R_m = 20.5 \text{ kg} / M_e \quad (2)$$

Calculate the mass ratio for the test.

It is assumed that the dummy has the same shoulder stiffness as the standard subject, and the stiffness ratio, R_k , is equal to 1.

The normalizing factors for force, time and displacement acceleration are given by,

$$R_f = (R_m R_k)^{\frac{1}{2}} \quad (3)$$

$$R_t = R_x = (R_m)^{\frac{1}{2}} (R_k)^{-\frac{1}{2}} \quad (4)$$

Normalize the force-time curve by multiplying each force value and each time value by their corresponding normalizing factors. Normalize the maximum shoulder to thoracic spine deflection by multiplying it by R_x .

A dummy with reasonable response characteristics will have a normalized force-time curve that lies within the proposed response corridor depicted in Figure 1 and a normalized maximum shoulder deflection that is between 34 and 41 mm.

5.0 REFERENCES

1. Bendjallal, F., Walisch, G., Fayon, A., and Tarriere, C., "APR Biomechanical Data", Nanterre, France, Jan., 1984.
2. Ewing, C. L., Thomas, D. J., Majewski, P. L., Black, R., and Lustik, L., "Measurement of Head, T1, and Pelvic Response to -Gx Impact Acceleration", SAE 770927, Twenty-First Stapp Car Crash Conference, Oct., 1977.
3. Mertz, H. J., "A Procedure for Normalizing Impact Response Data", SAE 840884, Warrendale, PA, May, 1984.

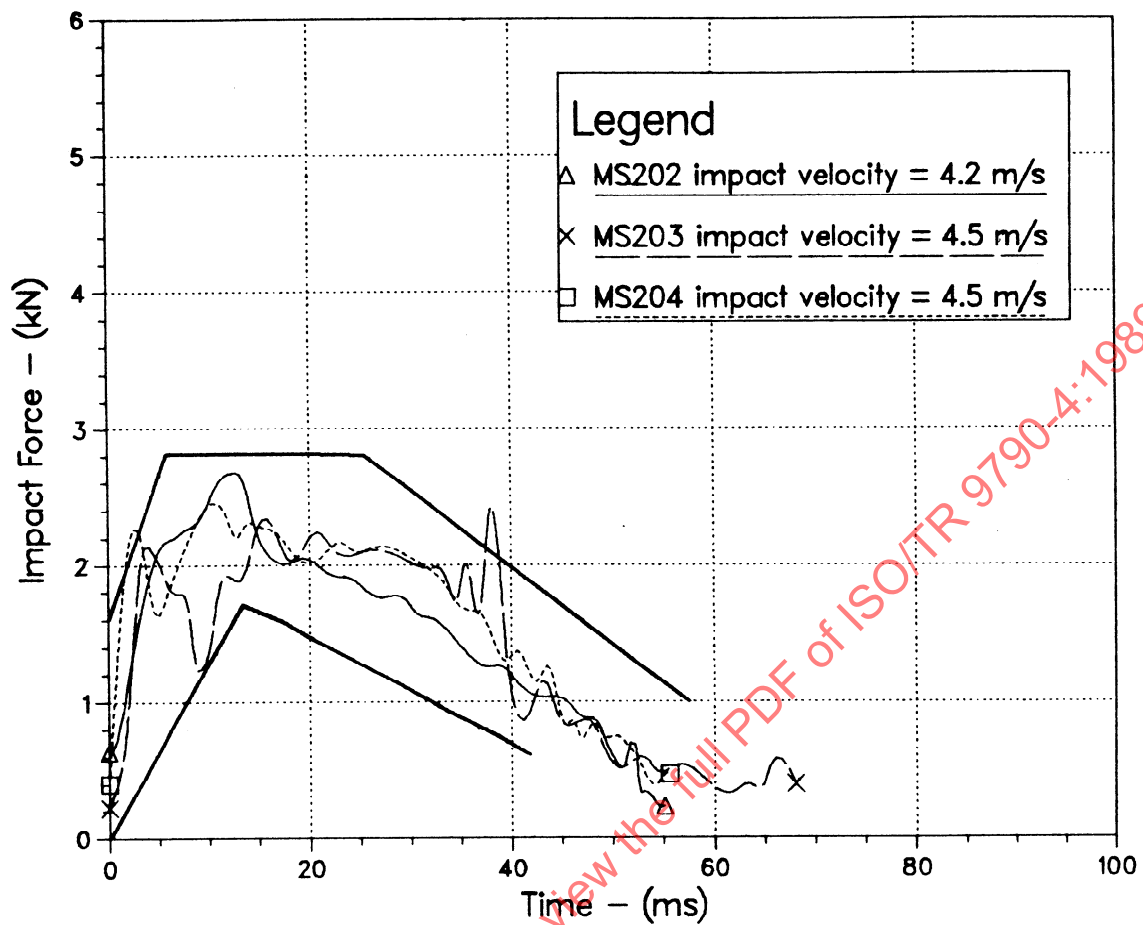


FIGURE 1. NORMALIZED LATERAL SHOULDER FORCE-TIME CURVES AND A PROPOSED CORRIDOR FOR A 4.5 m/s IMPACT DELIVERED BY A 23 kg RIGID CYLINDER.

APPENDIX A

ANALYSIS OF ASSOCIATION PEUGEOT-RENAULT
LATERAL SHOULDER IMPACT DATA

This appendix describes the application of the normalization techniques of Mertz (3) to the lateral shoulder impact data provided by the Association Peugeot-Renault (1).

A.1 Original Data

Researchers of the Association Peugeot-Renault subjected 4 cadavers to lateral impacts delivered to the shoulder by the flat end of a 23 kg rigid cylinder ($D = 150$ mm). Each cadaver was seated on a hardwood horizontal surface with a vertical backrest. The cadaver's hands were placed on its lap and the arm on the impacted side was suspended as if supported by an armrest. The impact was delivered laterally to the shoulder for Tests MS 201, MS 202, and MS 203. The impact for Test MS 204 was delivered at an angle of 15° forward of lateral, as defined in Figure 1. The force and acceleration of the impactor, the acceleration of the thoracic spine and the deflection of the shoulder relative to the thoracic spine were measured for each test. Following each test, the cadaver was autopsied for fractures of the ribs, clavicle, or scapula.

Table 1 provides a summary of the weights and thoracic depths of the cadavers. The impact angle defined in Figure 1, the impact velocity and the maximum deflection of the shoulder relative to the thoracic spine are also given. The force-time plots for the loads applied to the cadaver's shoulders are shown in Figure 2. Acceleration-time plots are not shown since they were not provided.

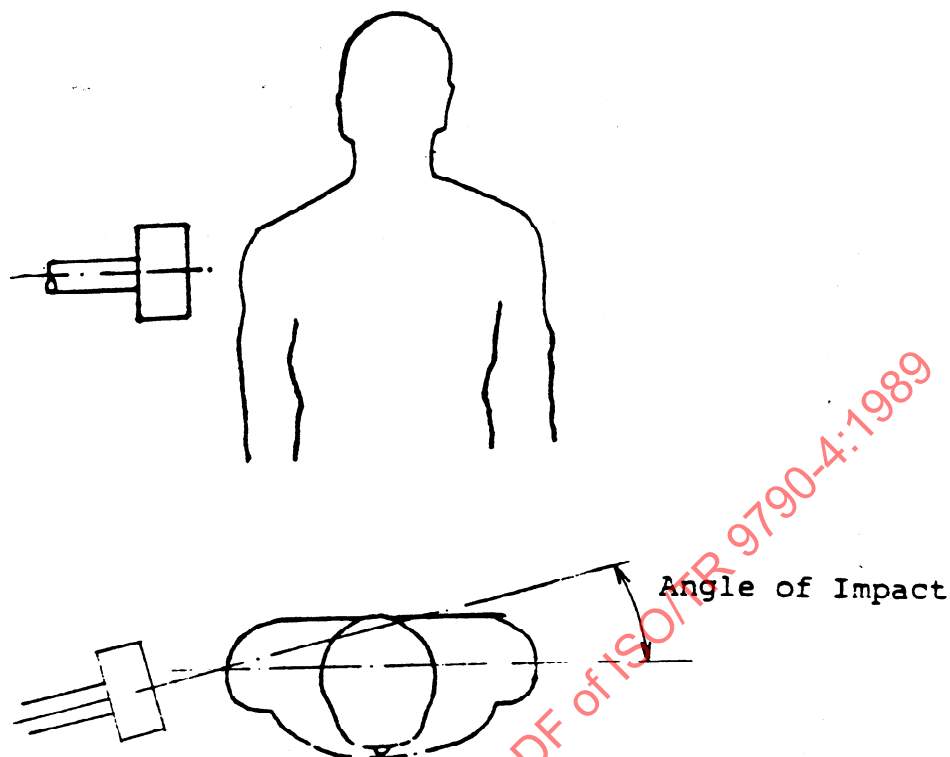


FIGURE 1. SHOULDER IMPACT TEST CONFIGURATION FOR TEST MS 204.

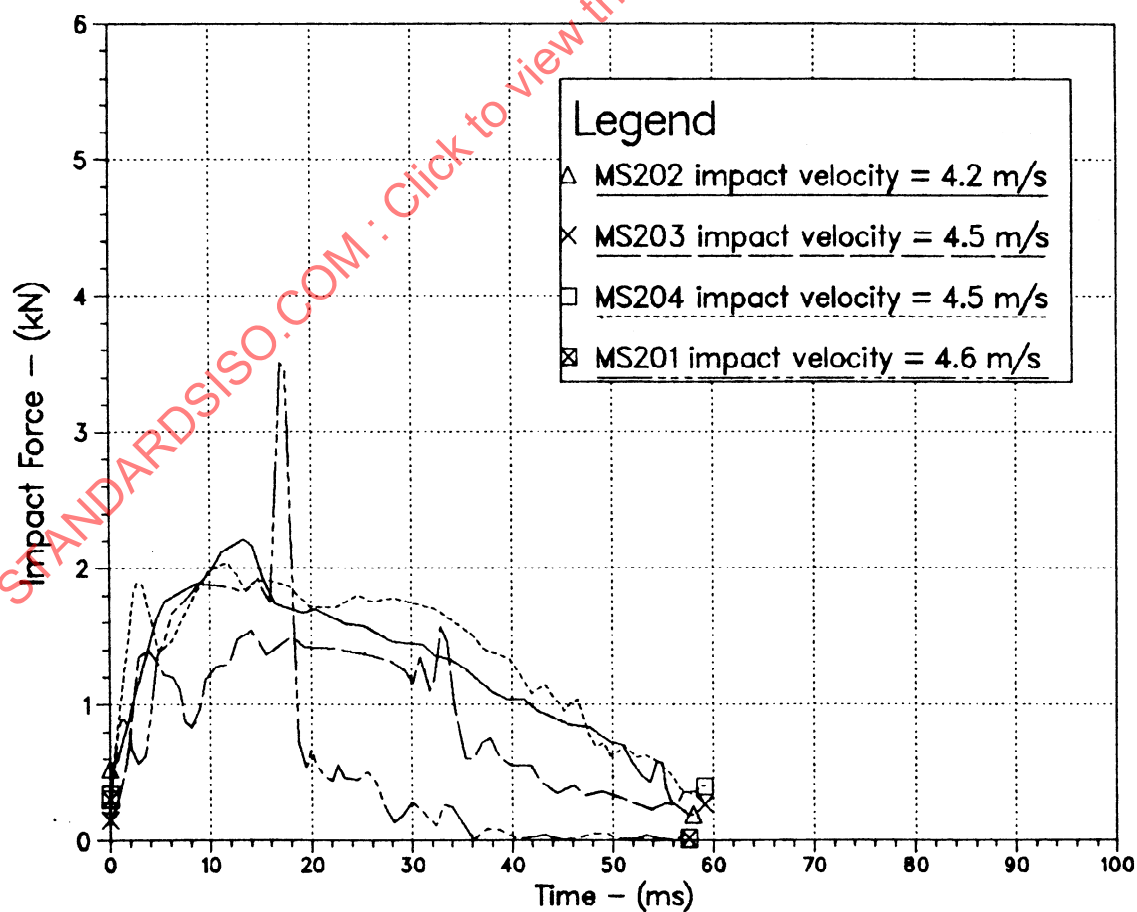


FIGURE 2. LATERAL SHOULDER FORCE-TIME CURVES FOR CADAVERS SUBJECTED TO IMPACTS DELIVERED BY A 23 KG RIGID CYLINDER (1).

TABLE 1. Cadaver Data, Test Conditions, and Test Results (1) for the Shoulder Impact Tests Performed by the Association Peugeot-Renault; and Effective Mass, Characteristic Ratios, and Normalizing Factors for the Shoulder Impact Data.

Test Number	Cadaver Data		Test Conditions		Test Results		Effective Mass		Characteristic Ratios			Normalizing Factors			
	Body Mass (kg)	Thoracic Depth (cm)	Impact Angle (°)	Impact Velocity (m/s)	Defl. (mm)	Impulse (Ns)	M _e (kg)	Percent Body Mass (%)	R _m	Mass Stiffness	R _k	R _f	Force	Time	Defl.
MS 202	52	18.5	0	4.2	34	74.6	17.8	34.2	1.15	1.28	1.21	.95	.95		
MS 203	49	18.0	0	4.5	37	53.7	11.9	24.3	1.72	1.31	1.50	1.15	1.15		
MS 204	56	18.5	15	4.5	-	82.1	18.2	32.5	1.13	1.28	1.20	.94	-		
MS 201	48	18.0	0	4.6	37	37.1	8.1	16.9	2.53	1.31	1.82	1.39	1.39		

NOTE: Average Percent of Body Mass = 27.0%.

Deflection Data for Test MS 204 is Not Available.

A.2 Normalized Data

The force-time curves of the impactor were digitized. The characteristic features of each curve were represented by approximately 50 points. The areas under the force-time curves were calculated using the trapezoidal method of integration and the results are given in Table 1 under the heading of Impulse. The acceleration-time plots and changes in velocity were not available. The impact velocity was used as an approximation of the change in velocity. The effective mass was estimated by,

$$M_e = [\int_0^T F dt] / (V_0) \quad (1)$$

where $\int_0^T F dt$ is the area under the force-time plot and V_0 is the impact velocity. The effective mass and percent of body mass for each cadaver are given in Table 1.

The average percent of body mass is 27.0%. The effective mass of a 50th percentile male was obtained by multiplying its body mass of 76 kg by 27.0%, giving an effective mass of 20.5 kg.

The mass ratio, R_m , is defined as,

$$R_m = M_s M_i^{-1} \quad (2)$$

where M_s is the effective mass of the standard subject and M_i is the effective mass of the i -th subject. For the data discussed here, Equation 2 becomes,

$$R_m = 20.5 \text{ kg} / M_i \quad (3)$$

The mass ratios for the cadavers are given in Table 1.

The stiffness ratio, R_k , is defined as,

$$R_k = K_s K_i^{-1} \quad (4)$$

where K_s is the stiffness of the standard subject and K_i is the stiffness of the i -th subject. Mertz (3) has shown that for geometrically similar structures with the same elastic modulus the stiffness is proportional to the characteristic length. Thus the stiffness ratio can be expressed as,

$$R_k = L_s L_i^{-1} \quad (5)$$

The characteristic length for the shoulder was chosen as the depth of the thorax. The thoracic depth of a 50th percentile male is 23.6 cm. Using $L_s = 23.6$ cm, Equation 5 becomes,

$$R_k = 23.6 \text{ cm} / L_i \quad (6)$$

The stiffness ratios for the cadavers are given in Table 1.

The normalizing factors for force, R_f , time, R_t , and deflection, R_x , are defined as,

$$R_f = (R_m R_k)^{\frac{1}{2}} \quad (7)$$

$$R_t = (R_m)^{\frac{1}{2}} (R_k)^{-\frac{1}{2}} \quad (8)$$

$$R_x = (R_m)^{\frac{1}{2}} (R_k)^{-\frac{1}{2}} \quad (9)$$

These normalizing factors for the cadaver impacts are listed in Table 1. The force and time factors were used to normalize the force-time curves shown in Figure 2. For a given impact, each force value was multiplied by its force normalizing factor and each time value was multiplied by its time normalizing factor. The resulting normalized force-time curves are shown in Figure 3.

A.3 Force-Time Response Requirements

The normalized force-time curves of the cadaver subjects should map onto a single curve representing the response of a standard cadaver subject.